

Monte Carlo dosimetric study of the Flexisource Co-60 high dose rate source

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Abstract

Purpose: Recently, a new HDR ⁶⁰Co brachytherapy source, Flexisource Co-60, has been developed (Nucletron B.V. Veenendaal, The Netherlands). This study aims to obtain dosimetric data for this source for its use in clinical practice as required by AAPM and ESTRO.

Material and methods: Two Monte Carlo radiation transport codes were used: Penelope2008 and GEANT4. The source was centrally-positioned in a 100 cm radius water phantom. Absorbed dose and collisional kerma were obtained using 0.01 cm (close) and 0.1 cm (far) sized voxels to provide high-resolution dosimetry near (far from) the source. Dose rate distributions obtained with the two Monte Carlo codes were compared.

Results and Discussion: Simulations performed with those two radiation transport codes showed an agreement typically within 0.2% for $r > 0.8$ cm and up to 2% closer to the source. Detailed results of dose distributions are being made available.

Conclusions: Dosimetric data are provided for the new Flexisource Co-60 source. These data are meant to be used in treatment planning systems in clinical practice.

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Purpose

According to the American Association of Physicist in Medicine (AAPM) and the European Society for Radiotherapy and Oncology (ESTRO) recommendations [1], in order to fulfil the dosimetric prerequisites, all sources to be used in clinical practice have to have a set of dosimetric parameters available based on the Radiation Therapy Committee Task Group No. 43 (TG-43) formalism [2,3]. The AAPM High Energy Brachytherapy Source Dosimetry Working Group (HEBD-WG) recommends [1] that this dataset must be based upon at least one experimental study and at least one Monte Carlo (MC) study of the model's source dosimetric parameters. For conventionally encapsulated sources similar in design to existing or previously existing ones, a single dosimetric study published in a peer-reviewed journal is sufficient. The high dose rate (HDR) ⁶⁰Co sources fall in this category. MC or experimental dosimetry (or both) methods may be used. These studies must be performed by investigators that are independent from the manufacturer and published in a peer-reviewed journal prior to the use of these isotopes in clinical practice.

The HEBD-WG is also concerned about the dosimetry in the near-source region where the influence of β electrons

and the lack of electronic equilibrium are frequently neglected [4-6]. Commercial treatment planning systems (TPS) allow direct introduction of tabulated dose rates from the literature using the TG-43 formalism. These TG-43 data are usually derived from MC radiation transport simulations, estimating absorbed dose by collisional kerma. Consequently, these data are provided at distances from the source capsule large enough to ensure that the equivalence of collisional kerma and dose is applicable. TPS extrapolate data outside the available TG-43 data range. In case of HDR ⁶⁰Co sources, kerma to dose differences are significant and source model specific [4]. Kerma extrapolation at short distances would not be necessary if TG-43 data were available with adequate range and spatial resolution that include source electron contributions to absorbed dose and account for electron disequilibrium.

High dose rate (HDR) brachytherapy ⁶⁰Co sources have been considered for use in clinical practice as an alternative for ¹⁹²Ir HDR sources [7]. A comparison between the radiological properties of cobalt and iridium HDR sources have been performed in reference [8]. Additionally to cost and logistics improvements due to the cobalt longer half life, clinical examples for intracavitary and interstitial applications show practically identical dose distributions.

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The main goal of this work is to present the TG-43 data and the 2D dose rate table in cylindrical coordinates for treatment planning and quality assurance purposes (QA) for the new Flexisource Co-60 HDR source model used by the Flexitron remote HDR afterloader (Nucletron B.V., Veenendaal, The Netherlands) in a consistent way that is valid at short and long distances. Such a source has not been studied and published previously.

Material and methods

The design and materials of the Flexisource Co-60 HDR source was provided by the manufacturer. The source design and dimensions are shown schematically in Fig. 1. It is composed of a central cylindrical active core made of metallic ⁶⁰Co with a density of 8.9 g/cm³, 3.5 mm in length and 0.5 mm in diameter. The active core is covered by a cylindrical 316L stainless steel (67% Fe, 11% Ni, 18% Cr, 2% Si, 2% Mn) layer of 0.9 mm of external diameter and a density of 8 g/cm³. For this study we considered 2 mm 316L steel cable with an effective density of 4.81 g/cm³ (measured from the inner clamp). The interstitial areas between the active element and the cover were considered to be filled with standard dry air.

MC methods for radiation transport simulations were used to study the dose rate distribution around the source. Different MC codes presented different physics models, different cross sections data, and dissimilar tracking methods in the transport of electrons. As dose at short distances from the source was required, where electronic disequilibrium conditions may be dosimetrically important, two different MC codes were used. These MC codes were Penelope2008 [9] and GEANT4 (version 9.3) [10], which have been successfully used for dosimetric studies in the field of the brachytherapy [4,11-15].

GEANT4 and Penelope2008 photon and electron cross-sections are based on the EPDL97 and EEDL97 cross sections libraries, respectively [16, 17]. However, Penelope2008 also considers the impulse approximation that accounts for Doppler broadening and binding effects [9]. Consequently, photoelectric effect, pair production and Rayleigh cross-sections used by both codes were the same, while Compton cross-sections in Penelope2008 differed from those of GEANT4. Possible influence on the dosimetric results by

using Penelope2008 with the Compton cross-sections of the EPDL97 library has been discussed elsewhere [14] and found to be negligible. The photon spectrum was taken from the NuDat database [18] as suggested in Ref. [19]. The number of photons N_γ generated in each simulation was as follows: Penelope2008 ($N_\gamma = 5 \times 10^9$), GEANT4 ($N_\gamma = 1 \times 10^9$ to obtain water kerma and $N_\gamma = 4 \times 10^9$ to calculate absorbed dose). The electron spectrum including β decay, internal conversion electrons (IC) and Auger electrons was not considered in the simulation since its effect over the total dose was known to be less than 1% at distances greater than 0.1 cm from the source surface [4]. In each disintegration, 2,0001 photons/(Bq s) were generated on average. However, due to the 10 keV cut-off used, the photon intensity was reduced to 1.9985 photons/(Bq s).

Dose to water contribution was calculated in Penelope2008 using the tally provided within the penEasy package [20], whereas in GEANT4 it was evaluated using a homemade routine with the function GetTotalEnergyDeposit of the GEANT4 toolkit. To estimate the collisional kerma, homemade routines using the linear track-length estimator [21] were developed for Penelope2008 and GEANT4. Dose and collisional kerma rate distributions were used to derive the final dosimetric parameters as a function of r at every polar angle sampled.

The source was located at the geometric center of a spherical liquid water phantom with 100 cm radius, to estimate dose to water and simulate unbounded phantom conditions for $r < 20$ cm [22]. Water composition and mass density were those recommended by the AAPM [3]. Due to the high energy of the ⁶⁰Co, the photon spectrum electronic equilibrium is not reached up to a distance of approximately 0.75 cm from the surface of the source [4]. Thus, the dose for small distances cannot be approximated by collisional kerma as is usually done for ¹⁹²Ir or ¹³⁷Cs sources. Differences between collisional kerma and dose at $r = 0.75$ cm are less than 0.5% and negligible at $r = 1$ cm [4]. Since the evaluation of collisional kerma was more efficient (reduced statistical uncertainty and improved numerical performance) we have considered absorbed dose to water for distances smaller than 0.75 cm and collisional kerma from 0.75 cm up to 20 cm. In order to provide adequate spatial resolution, the cells were 0.01 cm in thickness for $r < 2$ cm from the source and a factor of 10 thicker for $2 \text{ cm} < r < 20$ cm, respec-

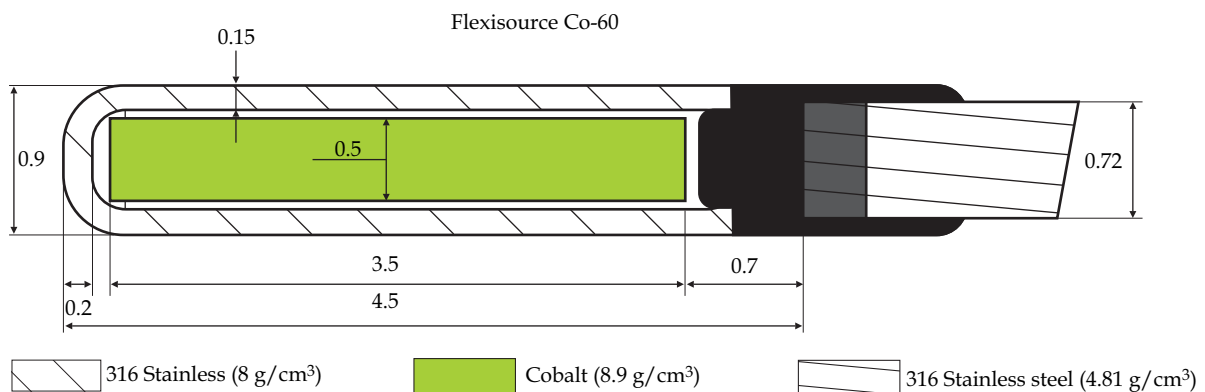


Fig. 1. Schematic design and dimensions of the model Flexisource Co-60 HDR source. Dimensions are given in mm

Table 1. Comparison of dose rate constant values calculated for similar ^{60}Co HDR sources

	L (cm)	Λ (cGy h $^{-1}$ U $^{-1}$)	Λ/G ($r = 1$ cm, $\theta = 90^\circ$) (cGy cm 2 h $^{-1}$ U $^{-1}$)
Flexisource Co-60 (This work)	0.35	1.085 \pm 0.003	1.096
BEBIG Multisource GK60M21 [10]	0.35	1.084 \pm 0.005	1.095
BEBIG Multisource Co0.A86 [12]	0.35	1.090 \pm 0.010	1.098
Ralstron Type 2 [8]	0.20	1.101 \pm 0.005	1.105
GZP6 source (Ch. 6) [13]	0.35	1.086 \pm 0.005	1.097
GZP6 source (Ch. 3/4) [13]	0.35	1.087 \pm 0.005	1.098

Table 2. Radial dose function calculated for the Flexisource Co-60 HDR source

r (cm)	$g_L(r)$
0.1	0.837
0.15	0.971
0.2	1.045
0.22	1.065
0.25	1.079
0.27	1.081
0.3	1.080
0.4	1.054
0.5	1.031
0.6	1.021
0.7	1.012
0.8	1.004
0.9	1.002
1	1.000
1.5	0.992
2	0.984
2.5	0.976
3	0.967
3.5	0.960
4	0.951
4.5	0.944
5	0.935
6	0.919
7	0.902
8	0.885
9	0.868
10	0.850
11	0.832
12	0.814
14	0.777
16	0.739
18	0.701
20	0.663

ctively. Collisional kerma and absorbed dose were obtained simultaneously in cylindrical (y,z) and spherical (r,θ) coordinates. Angular sampling was taken every 2° .

Additional simulations were performed to obtain S_K with the source surrounded by vacuum, except for a small cylindrical air cell of 0.1 cm in diameter and 0.1 cm in height at $r = 10$ cm, as recommended by AAPM [3]. Mass-energy absorption coefficients in water and air were consistently derived for each code and used to calculate the collisional kerma.

Results

The dose rate distribution $\dot{D}(r,\theta)$ for the Flexisource Co-60 HDR source model constructed as described in Sect. Material and Methods was used to derive the TG-43 dosimetry parameters with $L = 0.35$ cm. Using Penelope2008 and GEANT4, an average of $\Lambda = 1.085 \pm 0.003$ cGy/(h U) (with $k = 1$) was obtained. Uncertainties are Type A only. These are similar to the consensus values published for other ^{60}Co sources, see Table 1. In Table 2 and 3 $g_L(r)$ and $F(r,\theta)$ are provided in 0.1 cm steps (or smaller) up to 1.0 cm from the source (to reproduce the dose distribution accurately at close distances) and in 0.5 cm and 1 cm steps up to 20 cm. Both functions were obtained as average results from Penelope2008 and GEANT4 codes. $F(r,\theta)$ was provided for all radial distances in 2° increments. An along-away table for QA purposes is also provided in Table 4.

Differences in using $\dot{D}(r,\theta)$ Penelope2008 and GEANT4 were within the statistical uncertainties (type A). These uncertainties were larger at $r < 1$ cm where absorbed dose were scored (between 0.5% at $r = 0.2$ cm and 1% at $r = 0.8$ cm) and lower at larger distances (below 0.1%) where the collisional kerma was used.

Discussions

In this study, we have compared our results with those obtained for other ^{60}Co sources discussed in the literature. Papagiannis *et al.* [23] used MC to obtain dose rate in water (30 cm in diameter water phantom) of the Ralstron Type-1, Type-2 and Type-3 source models manufactured by Shimazdu Corporation (Japan) and used in the Ralstron remote afterloader. Their configuration consists of two active pellets (cylinders 1 mm \times 1 mm) either in contact (Type-2), 9 mm (Type-1) or 11 mm apart (Type-3). All three models have a 3 mm external diameter. Kerma-dose approxima-

Table 3. Anisotropy function calculated for the Flexisource Co-60 HDR source

θ°	r/cm																
	0.1	0.15	0.2	0.22	0.25	0.27	0.3	0.4	0.5	0.6	0.7	0.8	0.9	1	1.5	2	2.5
0	NaN	NaN	NaN	NaN	0.653	0.696	0.765	0.920	0.969	0.955	0.963	0.945	0.948	0.950	0.948	0.952	0.952
2	NaN	NaN	NaN	NaN	0.659	0.700	0.765	0.917	0.971	0.965	0.968	0.955	0.955	0.956	0.954	0.956	0.955
4	NaN	NaN	NaN	NaN	0.665	0.704	0.765	0.915	0.973	0.975	0.974	0.960	0.961	0.961	0.960	0.959	0.959
6	NaN	NaN	NaN	NaN	0.663	0.706	0.770	0.923	0.975	0.976	0.975	0.962	0.961	0.961	0.960	0.959	0.960
8	NaN	NaN	NaN	NaN	0.667	0.711	0.775	0.929	0.977	0.974	0.977	0.965	0.963	0.964	0.963	0.963	0.963
10	NaN	NaN	NaN	NaN	0.675	0.717	0.781	0.935	0.977	0.976	0.975	0.969	0.969	0.969	0.967	0.967	0.967
12	NaN	NaN	NaN	NaN	0.685	0.727	0.790	0.936	0.979	0.978	0.983	0.972	0.971	0.972	0.972	0.971	0.972
14	NaN	NaN	NaN	0.610	0.690	0.736	0.800	0.944	0.983	0.980	0.986	0.976	0.975	0.976	0.975	0.975	0.975
16	NaN	NaN	0.596	0.637	0.704	0.749	0.811	0.944	0.986	0.984	0.988	0.978	0.978	0.978	0.978	0.977	0.978
18	NaN	NaN	0.633	0.665	0.721	0.762	0.821	0.950	0.989	0.990	0.990	0.982	0.981	0.981	0.981	0.981	0.981
20	NaN	NaN	0.675	0.695	0.743	0.780	0.834	0.954	0.992	0.992	0.992	0.984	0.984	0.984	0.985	0.984	0.984
22	NaN	0.703	0.706	0.723	0.764	0.797	0.847	0.957	0.993	0.991	0.989	0.986	0.986	0.986	0.985	0.985	0.986
24	NaN	0.724	0.732	0.748	0.785	0.815	0.861	0.964	0.994	0.991	0.991	0.987	0.988	0.988	0.988	0.987	0.988
26	NaN	0.742	0.757	0.772	0.806	0.833	0.874	0.970	0.997	0.994	0.993	0.989	0.989	0.989	0.989	0.988	0.989
28	NaN	0.764	0.779	0.793	0.824	0.848	0.886	0.975	0.997	0.993	0.995	0.991	0.991	0.991	0.990	0.990	0.990
30	NaN	0.781	0.800	0.814	0.842	0.864	0.898	0.977	0.996	0.994	0.998	0.992	0.992	0.992	0.992	0.991	0.992
32	NaN	0.795	0.818	0.832	0.859	0.879	0.910	0.981	0.998	0.995	0.999	0.993	0.992	0.992	0.992	0.992	0.992
34	NaN	0.813	0.835	0.849	0.874	0.893	0.921	0.986	1.000	0.994	0.998	0.993	0.993	0.993	0.994	0.993	0.993
36	NaN	0.830	0.852	0.864	0.888	0.905	0.930	0.990	1.001	0.997	0.997	0.995	0.995	0.995	0.994	0.994	0.994
38	0.824	0.843	0.866	0.877	0.898	0.914	0.937	0.991	1.002	0.997	0.998	0.995	0.995	0.996	0.995	0.995	0.995
40	0.839	0.857	0.881	0.892	0.910	0.924	0.945	0.995	1.005	1.000	1.003	0.995	0.995	0.996	0.995	0.995	0.995
42	0.855	0.872	0.893	0.904	0.921	0.933	0.953	0.997	1.006	1.001	1.001	0.996	0.996	0.996	0.996	0.996	0.996
44	0.875	0.882	0.904	0.913	0.929	0.940	0.959	0.999	1.005	0.999	1.000	0.996	0.997	0.997	0.997	0.996	0.996
46	0.892	0.895	0.914	0.924	0.939	0.949	0.965	1.002	1.002	1.001	1.003	0.997	0.997	0.998	0.997	0.996	0.996
48	0.905	0.905	0.923	0.932	0.946	0.955	0.968	1.003	1.003	1.000	0.998	0.997	0.998	0.998	0.998	0.997	0.998
50	0.915	0.916	0.932	0.939	0.952	0.962	0.975	1.001	1.003	0.999	1.004	0.998	0.998	0.998	0.998	0.998	0.997
52	0.924	0.924	0.938	0.946	0.958	0.966	0.978	0.999	1.004	0.999	1.005	0.998	0.998	0.998	0.998	0.998	0.998
54	0.933	0.932	0.946	0.953	0.965	0.973	0.983	1.000	1.001	1.001	1.004	0.998	0.999	0.999	0.999	0.998	0.998
56	0.935	0.942	0.954	0.959	0.968	0.974	0.984	1.003	1.004	1.001	1.003	0.998	0.999	0.999	0.999	0.998	0.998
58	0.943	0.948	0.960	0.966	0.974	0.979	0.987	1.004	1.005	1.000	1.003	0.998	0.999	1.000	0.999	0.998	0.998
60	0.953	0.955	0.964	0.969	0.978	0.983	0.990	1.004	1.002	1.000	1.003	0.999	0.999	0.999	0.999	0.999	0.999
62	0.960	0.959	0.969	0.973	0.980	0.984	0.991	1.003	1.002	1.001	1.003	0.998	1.000	1.000	0.999	0.999	0.999
64	0.964	0.966	0.973	0.976	0.981	0.985	0.991	1.003	1.002	1.001	1.005	0.999	1.000	1.000	1.000	0.999	0.999
66	0.972	0.973	0.978	0.980	0.985	0.989	0.994	1.001	1.003	1.001	1.003	0.999	0.999	0.999	0.999	0.999	0.999
68	0.979	0.976	0.981	0.984	0.988	0.991	0.994	1.003	1.003	1.003	1.004	0.999	1.000	1.000	1.000	0.999	0.999
70	0.983	0.981	0.984	0.986	0.991	0.994	0.997	1.002	1.001	0.999	1.003	0.999	1.000	1.000	1.000	0.999	0.999
72	0.987	0.983	0.987	0.989	0.992	0.995	0.998	1.001	1.002	1.001	1.005	1.000	1.000	1.000	1.000	1.000	1.000
74	0.993	0.985	0.990	0.992	0.995	0.997	1.000	1.001	1.001	1.003	1.002	1.000	1.000	1.000	0.999	0.999	0.999
76	0.995	0.991	0.994	0.995	0.996	0.997	1.000	1.000	1.001	1.002	1.000	1.000	1.000	1.001	1.000	0.999	0.999
78	0.998	0.990	0.993	0.995	0.997	0.998	1.000	1.001	0.999	1.003	1.001	1.000	1.000	1.000	1.000	0.999	1.000
80	1.001	0.994	0.996	0.997	0.998	0.999	1.000	1.001	0.999	1.000	1.003	1.000	1.000	1.000	0.999	0.999	0.999
82	1.005	0.995	0.996	0.997	0.998	0.998	1.000	1.000	0.999	1.000	1.003	1.000	1.000	1.000	1.000	1.000	1.000
84	1.004	0.995	0.996	0.997	0.999	0.999	0.999	1.000	1.000	1.001	1.004	1.000	1.000	1.000	1.000	0.999	0.999
86	1.006	0.997	0.998	0.998	0.998	0.998	0.999	0.999	0.999	1.003	1.003	1.000	1.000	1.000	1.000	0.999	0.999
88	1.008	0.999	1.000	0.999	0.998	0.998	0.998	0.998	1.002	1.002	1.005	1.000	1.001	1.001	1.000	1.000	1.000

Table 3. Cont.

θ°	<i>r/cm</i>															
	3	3.5	4	4.5	5	6	7	8	9	10	11	12	14	16.	18	20
0	0.953	0.952	0.954	0.954	0.955	0.956	0.957	0.960	0.961	0.961	0.963	0.963	0.966	0.967	0.969	0.986
2	0.956	0.956	0.957	0.957	0.958	0.959	0.960	0.962	0.962	0.963	0.965	0.965	0.967	0.968	0.970	0.979
4	0.960	0.960	0.960	0.960	0.961	0.962	0.963	0.964	0.964	0.965	0.966	0.967	0.968	0.969	0.971	0.971
6	0.960	0.960	0.961	0.961	0.962	0.962	0.963	0.963	0.964	0.965	0.966	0.967	0.967	0.969	0.970	0.971
8	0.964	0.964	0.965	0.965	0.966	0.966	0.967	0.968	0.968	0.969	0.969	0.970	0.971	0.972	0.973	0.973
10	0.968	0.968	0.968	0.969	0.969	0.969	0.970	0.970	0.971	0.972	0.972	0.973	0.973	0.974	0.975	0.976
12	0.972	0.972	0.973	0.973	0.973	0.974	0.975	0.975	0.975	0.976	0.976	0.977	0.977	0.978	0.979	0.979
14	0.976	0.976	0.976	0.976	0.976	0.977	0.977	0.978	0.978	0.978	0.979	0.979	0.980	0.980	0.981	0.981
16	0.978	0.978	0.978	0.979	0.979	0.979	0.980	0.980	0.980	0.980	0.981	0.981	0.981	0.982	0.982	0.982
18	0.981	0.981	0.982	0.982	0.982	0.983	0.983	0.983	0.983	0.983	0.984	0.984	0.984	0.985	0.985	0.985
20	0.984	0.984	0.985	0.985	0.985	0.985	0.986	0.986	0.986	0.986	0.986	0.987	0.986	0.987	0.987	0.988
22	0.986	0.986	0.986	0.986	0.986	0.986	0.987	0.987	0.987	0.987	0.987	0.987	0.987	0.988	0.988	0.988
24	0.988	0.988	0.988	0.988	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.990	0.990
26	0.989	0.989	0.989	0.989	0.989	0.990	0.990	0.990	0.990	0.990	0.990	0.990	0.990	0.991	0.991	0.990
28	0.990	0.990	0.991	0.990	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.992	0.992
30	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.993	0.993	0.993	0.993
32	0.992	0.992	0.992	0.992	0.992	0.993	0.993	0.993	0.992	0.993	0.993	0.993	0.993	0.993	0.993	0.993
34	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.995	0.994
36	0.994	0.994	0.995	0.994	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995
38	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995
40	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995
42	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996
44	0.996	0.996	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997
46	0.996	0.996	0.997	0.997	0.996	0.997	0.997	0.997	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996
48	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998
50	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998
52	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
54	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.999	0.998	0.998	0.998	0.999	0.998
56	0.998	0.998	0.999	0.999	0.999	0.999	0.999	0.998	0.998	0.999	0.999	0.999	0.999	0.999	0.999	0.999
58	0.999	0.998	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
60	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
62	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
64	0.999	0.999	1.000	0.999	0.999	1.000	1.000	0.999	0.999	0.999	1.000	0.999	1.000	1.000	1.000	0.999
66	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
68	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	1.000	0.999
70	0.999	0.999	1.000	0.999	1.000	1.000	1.000	1.000	0.999	1.000	1.000	1.000	1.000	1.000	1.000	1.000
72	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
74	0.999	0.999	0.999	0.999	0.999	0.999	1.000	0.999	0.999	0.999	0.999	0.999	0.999	0.999	1.000	0.999
76	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
78	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	0.999	1.000	1.000
80	0.999	0.999	0.999	0.999	0.999	0.999	1.000	0.999	0.999	0.999	0.999	0.999	1.000	0.999	0.999	0.999
82	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
84	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	0.999	1.000	0.999	0.999	1.000	1.000	1.000	1.000
86	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
88	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000

Table 3. Cont.

θ°	r/cm																
	0.1	0.15	0.2	0.22	0.25	0.27	0.3	0.4	0.5	0.6	0.7	0.8	0.9	1	1.5	2	2.5
90	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
92	1.005	0.999	1.001	1.002	1.001	1.001	1.001	1.001	1.002	1.001	1.004	1.000	1.000	1.000	1.000	1.000	1.000
94	1.006	0.998	1.000	1.000	1.001	1.001	1.001	1.000	1.001	1.001	1.005	1.000	1.000	1.001	1.000	1.000	1.000
96	1.006	0.997	0.998	0.999	1.000	1.001	1.001	1.000	1.000	1.000	1.003	0.999	1.000	1.001	1.000	0.999	1.000
98	1.002	0.994	0.997	0.998	1.000	1.000	1.000	1.000	1.000	1.001	1.003	1.000	1.000	1.001	1.000	1.000	1.000
100	0.997	0.994	0.996	0.998	0.999	1.000	1.001	1.003	1.001	1.001	1.005	1.000	1.000	1.000	1.000	0.999	0.999
102	0.997	0.991	0.994	0.995	0.997	0.998	1.000	1.001	1.002	1.002	1.007	0.999	1.001	1.001	1.000	1.000	1.000
104	0.994	0.990	0.993	0.994	0.996	0.997	1.000	1.002	1.001	0.999	1.005	1.000	1.000	1.000	1.000	0.999	1.000
106	0.992	0.987	0.992	0.993	0.996	0.997	0.999	1.003	1.001	1.000	1.004	0.999	1.000	1.000	1.000	1.000	1.000
108	0.988	0.984	0.990	0.992	0.995	0.996	0.999	1.005	1.001	1.000	1.002	1.000	1.000	1.000	1.000	0.999	1.000
110	0.986	0.982	0.988	0.990	0.993	0.997	1.001	1.004	1.002	1.002	1.004	1.000	1.000	1.000	1.000	0.999	0.999
112	0.977	0.976	0.984	0.987	0.991	0.994	0.998	1.005	1.002	1.001	1.002	1.000	1.000	1.001	1.000	0.999	0.999
114	0.976	0.972	0.978	0.981	0.987	0.991	0.998	1.004	1.003	0.999	1.004	0.999	1.000	1.000	0.999	0.999	0.999
116	0.969	0.967	0.978	0.982	0.988	0.991	0.996	1.005	1.005	1.000	1.005	1.000	0.999	1.000	1.000	0.999	0.999
118	0.964	0.963	0.973	0.977	0.983	0.988	0.995	1.005	1.004	1.001	1.007	0.999	0.999	1.000	0.999	0.999	0.999
120	0.953	0.957	0.970	0.975	0.981	0.986	0.993	1.007	1.004	1.002	1.005	0.999	0.999	0.999	0.999	0.999	0.999
122	0.943	0.949	0.965	0.971	0.980	0.985	0.993	1.005	1.003	1.002	1.003	0.998	0.999	0.999	0.999	0.998	0.998
124	0.938	0.943	0.959	0.966	0.976	0.983	0.993	1.005	0.999	1.002	1.003	0.999	1.000	1.000	0.999	0.999	0.999
126	0.934	0.936	0.953	0.961	0.972	0.979	0.990	1.005	1.000	1.001	1.003	0.998	0.999	0.999	0.999	0.998	0.998
128	0.925	0.928	0.945	0.953	0.965	0.974	0.988	1.005	1.003	0.998	1.002	0.998	0.999	0.999	0.998	0.998	0.998
130	0.915	0.918	0.939	0.947	0.961	0.971	0.985	1.006	1.001	1.000	1.002	0.998	0.998	0.999	0.999	0.998	0.998
132	0.901	0.910	0.933	0.943	0.957	0.967	0.981	1.005	1.004	1.000	1.003	0.998	0.998	0.999	0.998	0.998	0.998
134	0.890	0.900	0.924	0.935	0.952	0.963	0.978	1.005	1.005	1.001	1.002	0.998	0.997	0.998	0.997	0.997	0.997
136	0.877	0.888	0.915	0.927	0.945	0.957	0.973	1.005	1.007	1.004	1.003	0.997	0.997	0.997	0.997	0.997	0.997
138	0.856	0.877	0.905	0.917	0.936	0.950	0.968	1.003	1.007	1.004	1.002	0.996	0.997	0.997	0.997	0.997	0.996
140	0.843	0.864	0.893	0.906	0.927	0.941	0.960	1.002	1.007	1.003	1.002	0.996	0.996	0.997	0.996	0.996	0.996
142	0.828	0.851	0.882	0.896	0.918	0.932	0.953	1.002	1.006	1.002	1.000	0.995	0.995	0.996	0.995	0.995	0.995
144	NaN	0.835	0.868	0.884	0.907	0.923	0.946	0.999	1.006	1.005	1.000	0.994	0.995	0.996	0.995	0.994	0.994
146	NaN	0.820	0.853	0.869	0.893	0.910	0.934	0.997	1.005	1.002	1.000	0.994	0.994	0.995	0.994	0.994	0.994
148	NaN	0.804	0.836	0.853	0.880	0.899	0.927	0.993	1.003	0.999	0.996	0.993	0.993	0.993	0.993	0.992	0.992
150	NaN	0.787	0.819	0.837	0.867	0.888	0.919	0.988	1.005	1.000	0.997	0.992	0.992	0.992	0.991	0.990	0.990
152	NaN	0.769	0.800	0.819	0.851	0.874	0.908	0.985	1.004	0.999	0.996	0.991	0.991	0.991	0.991	0.991	0.991
154	NaN	0.749	0.781	0.800	0.834	0.859	0.895	0.984	1.004	0.998	0.996	0.989	0.990	0.991	0.989	0.988	0.988
156	NaN	0.729	0.760	0.780	0.816	0.843	0.882	0.974	1.002	0.997	0.996	0.987	0.987	0.987	0.987	0.987	0.987
158	NaN	0.707	0.735	0.757	0.796	0.824	0.866	0.966	0.996	0.993	0.992	0.985	0.985	0.985	0.985	0.984	0.984
160	NaN	NaN	0.707	0.730	0.771	0.803	0.851	0.959	0.995	0.992	0.990	0.983	0.982	0.983	0.982	0.981	0.981
162	NaN	NaN	0.675	0.701	0.746	0.781	0.835	0.954	0.993	0.992	0.986	0.979	0.978	0.979	0.978	0.977	0.977
164	NaN	NaN	0.638	0.669	0.721	0.759	0.816	0.949	0.984	0.983	0.982	0.974	0.974	0.974	0.973	0.973	0.973
166	NaN	NaN	NaN	0.632	0.691	0.734	0.799	0.942	0.975	0.980	0.978	0.969	0.968	0.968	0.967	0.966	0.967
168	NaN	NaN	NaN	NaN	0.661	0.708	0.778	0.935	0.973	0.972	0.966	0.961	0.960	0.960	0.960	0.960	0.960
170	NaN	NaN	NaN	NaN	NaN	NaN	0.775	0.927	0.961	0.960	0.963	0.951	0.950	0.950	0.949	0.948	0.949
172	NaN	NaN	NaN	NaN	NaN	NaN	NaN	0.921	0.949	0.942	0.951	0.940	0.934	0.934	0.933	0.934	0.935
174	NaN	NaN	NaN	NaN	NaN	NaN	NaN	NaN	0.929	0.927	0.939	0.926	0.918	0.918	0.918	0.918	0.919
176	NaN	NaN	NaN	NaN	NaN	NaN	NaN	NaN	0.921	0.922	0.924	0.910	0.897	0.898	0.899	0.899	0.901
178	NaN	NaN	NaN	NaN	NaN	NaN	NaN	NaN	0.946	0.904	0.928	0.900	0.878	0.879	0.881	0.882	0.884
180	NaN	NaN	NaN	NaN	NaN	NaN	NaN	NaN	0.972	0.886	0.932	0.898	0.858	0.861	0.863	0.864	0.867

Table 3. Cont.

θ°	r/cm															
	3	3.5	4	4.5	5	6	7	8	9	10	11	12	14	16.	18	20
90	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
92	1.000	1.000	1.000	1.000	1.001	1.001	1.001	1.000	1.000	1.001	1.001	1.001	1.000	1.000	1.000	1.000
94	1.000	1.000	1.000	1.000	1.000	1.000	1.001	1.001	1.000	1.000	1.000	1.000	1.001	1.000	1.000	1.001
96	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	0.999	1.000	1.000	0.999	0.999	0.999	1.000	1.000
98	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
100	1.000	0.999	1.000	1.000	1.000	1.000	1.000	1.000	0.999	1.000	1.000	1.000	0.999	1.000	0.999	1.000
102	1.000	1.001	1.001	1.001	1.001	1.001	1.001	1.001	1.000	1.001	1.001	1.000	1.000	1.000	1.001	1.001
104	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
106	1.000	1.000	1.001	1.001	1.000	1.001	1.001	1.001	1.001	1.001	1.001	1.001	1.001	1.001	1.001	1.001
108	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
110	0.999	0.999	0.999	0.999	1.000	1.000	1.000	1.000	0.999	1.000	1.000	1.000	1.000	0.999	1.000	1.000
112	0.999	0.999	1.000	1.000	0.999	1.000	1.000	1.000	0.999	1.000	1.000	1.000	1.000	1.000	1.000	1.000
114	1.000	0.999	0.999	1.000	1.000	1.000	1.000	0.999	1.000	1.000	1.000	1.000	1.000	0.999	0.999	0.999
116	0.999	0.999	0.999	0.999	0.999	0.999	1.000	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
118	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
120	0.999	0.999	0.999	0.999	0.999	0.999	1.000	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
122	0.998	0.998	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.998	0.999	0.999	0.999	0.999
124	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999	0.999
126	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998
128	0.998	0.998	0.998	0.998	0.998	0.999	0.999	0.999	0.998	0.999	0.998	0.999	0.999	0.999	0.998	0.998
130	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998
132	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.998	0.997	0.997	0.997
134	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997
136	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.997	0.996	0.997	0.997	0.997	0.997	0.997	0.997	0.997
138	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996
140	0.996	0.996	0.996	0.996	0.996	0.997	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996	0.996
142	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.994	0.995	0.995	0.995	0.995	0.995	0.994	0.995
144	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995	0.995
146	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994	0.994
148	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992	0.992
150	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991
152	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.991	0.992	0.992	0.991	0.991	0.991	0.992	0.992
154	0.988	0.988	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989	0.989
156	0.987	0.987	0.987	0.987	0.987	0.987	0.987	0.987	0.987	0.987	0.987	0.987	0.987	0.988	0.988	0.988
158	0.984	0.984	0.984	0.984	0.984	0.985	0.985	0.985	0.985	0.985	0.985	0.985	0.986	0.986	0.986	0.986
160	0.981	0.982	0.982	0.982	0.982	0.982	0.983	0.982	0.983	0.983	0.983	0.983	0.983	0.984	0.984	0.984
162	0.977	0.977	0.977	0.977	0.978	0.978	0.978	0.979	0.978	0.979	0.979	0.979	0.979	0.980	0.980	0.981
164	0.973	0.974	0.974	0.974	0.974	0.975	0.975	0.975	0.976	0.976	0.976	0.977	0.978	0.978	0.979	0.979
166	0.967	0.967	0.967	0.968	0.968	0.969	0.969	0.970	0.970	0.971	0.971	0.972	0.972	0.973	0.973	0.974
168	0.961	0.961	0.961	0.962	0.962	0.963	0.964	0.964	0.965	0.966	0.966	0.967	0.967	0.968	0.969	0.970
170	0.950	0.950	0.951	0.951	0.952	0.953	0.954	0.955	0.956	0.957	0.958	0.958	0.960	0.961	0.963	0.963
172	0.936	0.936	0.937	0.938	0.939	0.940	0.942	0.943	0.944	0.945	0.947	0.948	0.950	0.951	0.953	0.955
174	0.921	0.922	0.923	0.924	0.925	0.927	0.929	0.931	0.932	0.935	0.936	0.937	0.940	0.942	0.944	0.946
176	0.902	0.904	0.906	0.907	0.909	0.911	0.914	0.916	0.918	0.920	0.923	0.925	0.928	0.932	0.935	0.935
178	0.886	0.887	0.889	0.891	0.893	0.896	0.899	0.902	0.904	0.907	0.908	0.911	0.915	0.919	0.922	0.914
180	0.869	0.871	0.872	0.876	0.877	0.880	0.884	0.889	0.890	0.893	0.893	0.897	0.902	0.906	0.908	0.893

Table 4. Along away (cGy h⁻¹ U⁻¹) table calculated for the Flexisource Co-60 HDR source for QA purposes

z/cm	y/cm														
	0.1	0.2	0.3	0.4	0.5	0.6	0.7	0.8	0.9	1	2	4	6	8	10
-10	0.00841	0.00842	0.00844	0.00846	0.00848	0.00850	0.00852	0.00855	0.00856	0.00859	0.00858	0.00778	0.00655	0.00531	0.00423
-8	0.0136	0.01365	0.01369	0.01373	0.01378	0.01381	0.01388	0.01392	0.01396	0.01398	0.01378	0.01178	0.00926	0.00705	0.00532
-6	0.0249	0.0251	0.0252	0.0253	0.0255	0.0256	0.0257	0.0258	0.0258	0.0258	0.0245	0.0188	0.01329	0.00929	0.00659
-4	0.0578	0.058	0.0589	0.059	0.060	0.060	0.060	0.060	0.060	0.059	0.051	0.0316	0.01890	0.01188	0.00789
-2	0.241	0.246	0.249	0.249	0.247	0.242	0.236	0.229	0.221	0.213	0.1326	0.0517	0.0250	0.01418	0.00891
-1	1.022	1.040	1.005	0.945	0.882	0.807	0.737	0.668	0.604	0.545	0.214	0.0611	0.0272	0.01489	0.00921
-0.9	1.293	1.287	1.232	1.144	1.047	0.945	0.847	0.757	0.675	0.603	0.223	0.0619	0.0273	0.01494	0.00922
-0.8	1.672	1.637	1.536	1.401	1.253	1.111	0.977	0.858	0.755	0.666	0.231	0.0625	0.0274	0.01498	0.00924
-0.7	2.23	2.15	1.965	1.741	1.513	1.308	1.128	0.973	0.842	0.733	0.239	0.0631	0.0276	0.01502	0.00926
-0.6	3.12	2.94	2.58	2.19	1.846	1.549	1.301	1.098	0.935	0.803	0.246	0.0636	0.0277	0.01506	0.00927
-0.5	NaN	4.21	3.48	2.80	2.26	1.826	1.492	1.232	1.032	0.873	0.253	0.0641	0.0277	0.01508	0.00928
-0.4	NaN	6.34	4.82	3.61	2.75	2.14	1.693	1.368	1.125	0.939	0.258	0.0645	0.0278	0.01510	0.00930
-0.3	NaN	10.01	6.73	4.60	3.29	2.46	1.891	1.494	1.210	0.998	0.263	0.0647	0.0279	0.01512	0.00930
-0.25	NaN	12.63	7.88	5.13	3.56	2.61	1.982	1.550	1.247	1.023	0.264	0.0648	0.0279	0.01513	0.00931
-0.2	NaN	15.69	9.06	5.64	3.82	2.74	2.06	1.598	1.278	1.044	0.266	0.0649	0.0279	0.01514	0.00931
-0.15	NaN	18.80	10.19	6.11	4.03	2.86	2.13	1.639	1.304	1.062	0.267	0.0650	0.0279	0.01514	0.00931
-0.1	NaN	21.4	11.11	6.48	4.20	2.95	2.18	1.668	1.323	1.074	0.268	0.0651	0.0279	0.01514	0.00931
-0.05	NaN	23.1	11.72	6.72	4.31	3.00	2.21	1.687	1.335	1.082	0.268	0.0651	0.0279	0.01514	0.00930
0	NaN	23.7	11.93	6.80	4.35	3.02	2.22	1.692	1.339	1.085	0.269	0.0651	0.0279	0.01514	0.00930
0.05	NaN	23.1	11.71	6.71	4.31	3.00	2.21	1.687	1.335	1.082	0.268	0.0651	0.0279	0.01514	0.00930
0.1	NaN	21.3	11.09	6.47	4.20	2.94	2.18	1.668	1.323	1.074	0.268	0.0651	0.0279	0.01514	0.00930
0.15	NaN	18.67	10.16	6.10	4.03	2.85	2.13	1.638	1.304	1.062	0.267	0.0650	0.0279	0.01513	0.00930
0.2	NaN	15.52	9.04	5.64	3.81	2.74	2.06	1.598	1.278	1.044	0.266	0.0649	0.0279	0.01513	0.00930
0.25	NaN	12.47	7.85	5.12	3.56	2.61	1.983	1.550	1.246	1.023	0.264	0.0648	0.0279	0.01512	0.00930
0.3	13.49	9.89	6.70	4.59	3.29	2.46	1.894	1.494	1.210	0.997	0.263	0.0647	0.0279	0.01512	0.00930
0.4	7.66	6.31	4.80	3.60	2.74	2.14	1.697	1.367	1.125	0.939	0.258	0.0644	0.0278	0.01510	0.00929
0.5	4.79	4.20	3.47	2.80	2.25	1.825	1.491	1.232	1.031	0.872	0.253	0.0640	0.0277	0.01508	0.00928
0.6	3.21	2.94	2.57	2.19	1.846	1.546	1.299	1.098	0.935	0.802	0.246	0.0636	0.0277	0.01505	0.00927
0.7	2.30	2.16	1.964	1.739	1.515	1.309	1.128	0.972	0.842	0.732	0.239	0.0631	0.0275	0.01501	0.00926
0.8	1.711	1.645	1.535	1.397	1.250	1.107	0.975	0.858	0.755	0.665	0.231	0.0625	0.0274	0.01497	0.00924
0.9	1.338	1.300	1.232	1.143	1.044	0.943	0.846	0.756	0.675	0.603	0.223	0.0618	0.0273	0.01493	0.00922
1	1.075	1.051	1.009	0.950	0.881	0.809	0.736	0.667	0.603	0.545	0.214	0.0611	0.0272	0.01489	0.00920
2	0.259	0.258	0.256	0.253	0.249	0.243	0.237	0.229	0.222	0.213	0.1326	0.0516	0.0250	0.01417	0.00891
4	0.0622	0.0623	0.0623	0.0621	0.0619	0.0616	0.0613	0.0609	0.0604	0.0598	0.0512	0.0316	0.01890	0.01189	0.00789
6	0.0267	0.0268	0.0268	0.0268	0.0267	0.0267	0.0266	0.0265	0.0264	0.0263	0.0246	0.01882	0.01330	0.00929	0.00659
8	0.01454	0.01448	0.01456	0.01455	0.01451	0.01453	0.01449	0.01447	0.01441	0.01440	0.01388	0.01178	0.00926	0.00705	0.00532
10	0.00892	0.00894	0.00893	0.00895	0.00894	0.00893	0.00894	0.00893	0.00891	0.00891	0.00870	0.00778	0.00655	0.00531	0.00423

tion was used. Papagiannis *et al.* [23] reported along-away dose rate tables and TG-43 dose parameters. Selvam *et al.* [24] have reported a systematic error for $y = 0.75$ cm in the away-along table of Papagiannis *et al.* for the type 2 source model.

Ballester *et al.* [13] studied the GK60M21 ⁶⁰Co (Eckert & Ziegler IBt-Bebig GmbH, Germany) using GEANT4 code

to obtain the dose rate distribution around this source in an unbounded water phantom. Only the gamma part of the ⁶⁰Co spectrum was considered. The β spectrum contribution to the dose was assumed to be insignificant. A cut-off energy of 10 keV was used for both photons and electrons. They scored kerma and dose separately to account for the electronic disequilibrium near the source. For points located

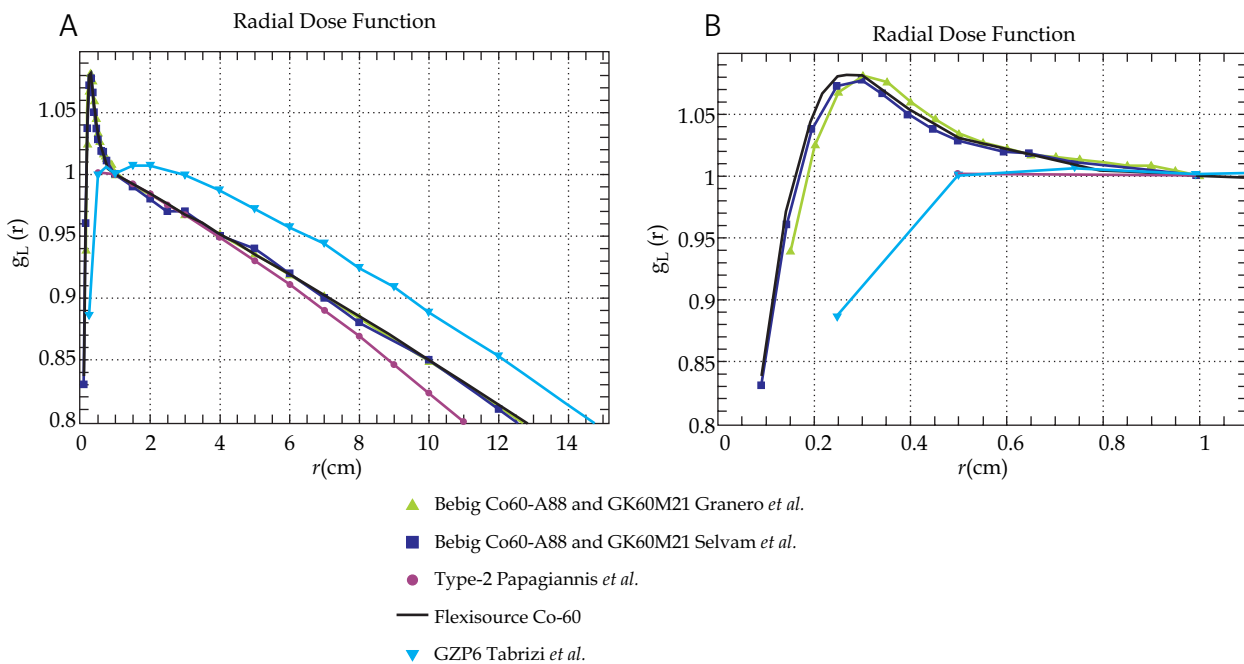


Fig. 2. A) Radial dose function of ^{60}Co source models. B) Zoom-in at short distances from the source where the electronic disequilibrium is located

at distances of less than 1 cm from the source they scored dose, while for distances where electronic equilibrium was achieved they scored kerma. They derived TG-43U1 parameters and an away-along table. Selvam *et al.* [25] reproduced the Ballester *et al.* [13] study, but using the EGSnrc code. They derived only an away-along table. The comparison of away-along tables from both studies reveals consistency between both studies except at $y = 0.25$ cm and $z = -0.25$, $z = 0$ and $z = 0.25$ cm were the Ballester *et al.* data had a typo.

Granero *et al.* [11] used GEANT4 MC code to obtain the dose rate distribution for the Co0.A86 ^{60}Co source model (Eckert & Ziegler IBt-Bebig GmbH, Germany) in an unbounded water phantom. The same type of study that the Ballester *et al.* [13], one of the GK60M21 source model described in the previous paragraph was done for the Co0.A86 source model. Selvam *et al.* [25] also reproduced the Granero *et al.* [11] study, but using the EGSnrc code, obtaining only an away-along table. The comparison of away-along tables from both studies reveals that at $(y = 0.25$ cm, $z = -0.25$ cm), $(y = 0.25$ cm, $z = 0$ cm), $(y = 0.25$ cm, $z = 0.25$ cm), the Granero *et al.* [11] data are underestimated. This is the same typo as in Ballester *et al.* data [13] for the GK60M21 source model.

Tabrizi *et al.* [26] studied two different ^{60}Co linear braid type sources available for the GZP6 remote afterloader (Nuclear Power Institute of China). These sources are composed of one active core made of metallic ^{60}Co with 3.5 mm length and 1.5 mm diameter, encapsulated in 0.1 mm titanium. The active core is covered by a cylindrical stainless steel cover of 0.5 mm external diameter and steel balls arranged along. The authors used the MCNP4C Monte Carlo code to

obtain the TG-43 dosimetric parameters together with along-away dose rate tables. Their radial dose function (see Fig. 2 in Tabrizi *et al.*) is inconsistent with other ^{60}Co source data and is difficult to understand from a physical point of view.

Papagianis *et al.* [23] showed that Λ/G ($r = 1$ cm, $\theta = 90^\circ$) values for different ^{60}Co source models are expected to match each other providing the spatial dependence of the dose rate constant as removed. In Table 1, it can be observed that the Flexisource Co-60 HDR source fits into this scheme.

$g_L(r)$ for the Flexisource Co-60 HDR source is compared in Fig. 2A with corresponding data to GK60M21 [13] and Co0.A86 [11] sources from BEBIG, Ralstron HDR Type 2 [23] from Shimazdu and GZP6 sources [26]. Figure 2B illustrates similarities/differences for $r < 1$ cm. The differences between Papagianis *et al.* data and those of the present study are due to the different phantom sizes used in the MC calculations. For the GZP6 source model data present an anomalous pattern.

Anisotropy function $F(r, \theta)$ is shown in Fig. 3 for $r \leq 1$ cm. At larger distances, $F(r, \theta)$ behave in a similar way as for $r = 1$ cm.

Conclusions

A dosimetric study of the Nucletron Flexisource Co-60 HDR source for which no published dosimetric data existed was performed. TG-43 parameters, dose rate constant, radial dose function and anisotropy function were provided together with a 2D along and away dose table. These datasets can be used either as an input for (or to validate) the TPS calculations essential for clinical practice.

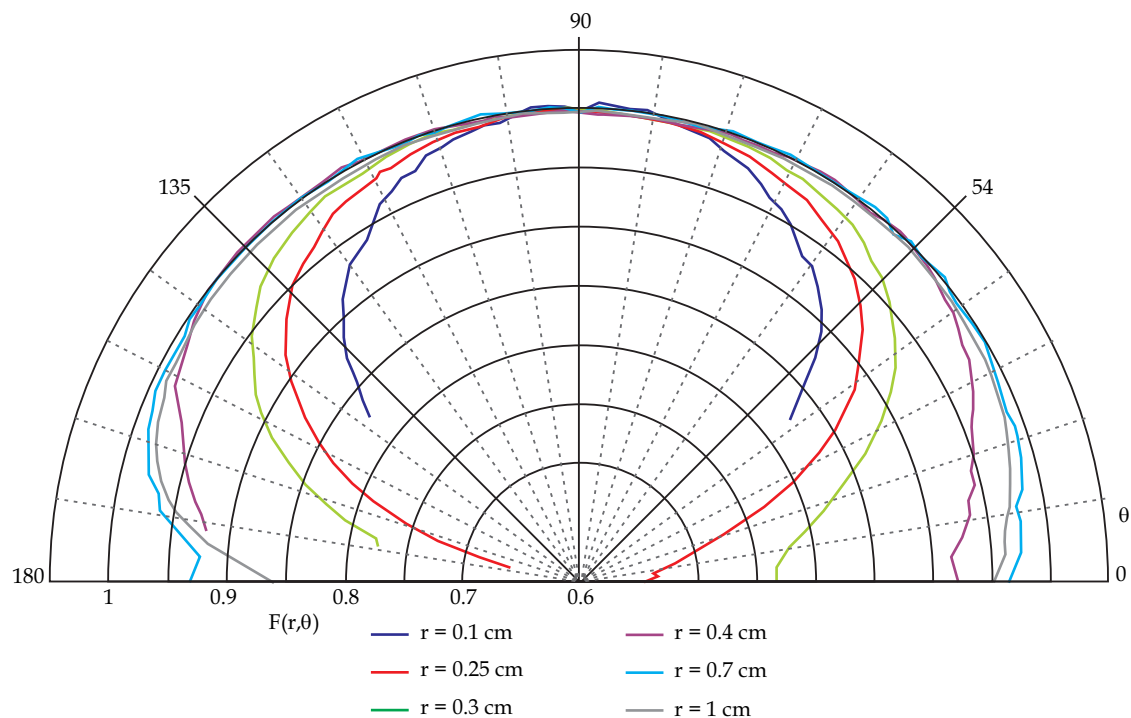


Fig. 3. Anisotropy function of the Flexisource Co-60 HDR source model for selected distances

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References

- Li Z, Das RK, DeWerd LA et al.; American Association of Physicists in Medicine (AAPM); European Society for Therapeutic Radiology and Oncology (ESTRO). Dosimetric prerequisites for routine clinical use of photon emitting brachytherapy sources with average energy higher than 50 keV. *Med Phys* 2007; 34: 37-40.
- Nath R, Anderson LL, Luxton G. et al. Dosimetry of interstitial brachytherapy sources: recommendations of the AAPM Radiation Therapy Committee Task Group No. 43. American Association of Physicists in Medicine. *Med Phys* 1995; 22: 209-234.
- Rivard MJ, Coursey BM, DeWerd LA et al. Update of AAPM Task Group No. 43 Report: A revised AAPM protocol for brachytherapy dose calculations. *Med Phys* 2004; 31: 633-674.
- Ballester F, Granero D, Pérez-Calatayud J et al. Evaluation of high-energy brachytherapy source electronic disequilibrium and dose from emitted electrons. *Med Phys* 2009; 36: 4250-4256.
- Baltas D, Karaiskos P, Papagiannis P et al. Beta versus gamma dosimetry close to Ir-192 brachytherapy sources. *Med Phys* 2001; 28: 1875-1882.
- Wang R, XA Li. A Monte Carlo calculation of dosimetric parameters of $^{90}\text{Sr}/^{90}\text{Y}$ and ^{192}Ir SS sources for intravascular brachytherapy. *Med Phys* 2000; 27: 2528-2535.
- Baltas D, Lymperopoulou G, Zamboglou N. On the use of HDR ^{60}Co source with the MammoSite radiation therapy system. *Med Phys* 2008; 35: 5263-5268.
- Richter J, Baier K, Flentje M. Comparison of 60-cobalt and 192-iridium sources in high dose rate afterloading brachytherapy. *Strahlenther Onkol* 2008; 184: 187-192.
- Salvat F, Fernández-Varea JM, Sempau J. PENELOPE-2008: a code system for Monte Carlo simulation of electron and photon transport, 2008. Issy-les-Moulineaux, France.
- GEANT4 Collaboration. GEANT4 – a simulation toolkit. *Nucl Instrum Methods Phys Res* 2003; 506: 250-303.
- Granero D, Perez-Calatayud J, Ballester F. Technical note: Dosimetric study of a new Co-60 source used in brachytherapy. *Med Phys* 2007; 34: 3485-3488.
- Granero D, Perez-Calatayud J, Pujades-Claumarchirant MC et al. Equivalent phantom sizes and shapes for brachytherapy dosimetric studies of ^{192}Ir and ^{137}Cs . *Med Phys* 2008; 35: 4872-4877.
- Ballester F, Granero D, Pérez-Calatayud J et al. Monte Carlo dosimetric study of the BEBIG Co-60 HDR source. *Phys Med Biol* 2005; 50: N309-N316.
- Granero D, Vijande J, Ballester F et al. Dosimetry revisited for the HDR ^{192}Ir brachytherapy source model mHDR-v2. *Med Phys* 2011; 38: 487-494.
- Meigooni AS, Wright C, Koona RA et al. TG-43 U1 based dosimetric characterization of model 67-6520 Cs-137 brachytherapy source. *Med Phys* 2009; 36: 4711-4719.
- Cullen DE, Hubbell JH, Kissel L. EPDL97: the Evaluated Photon Data Library, '97 Version, 1997, University of California, Lawrence Livermore National Laboratory: Livermore, CA.
- Cullen DE, Perkins ST, Seltzer SM. Tables and graphs of electron-interaction cross-sections from 10 eV to 100 GeV derived from the LLNL Evaluated Electron Data Library (EEDL) Z=1-100, 2001, Lawrence Livermore National Laboratory.
- NUDAT 2.5, National Nuclear Data Center, 2010, Brookhaven National Laboratory.
- Rivard MJ, Granero D, Perez-Calatayud J et al. Influence of photon energy spectra from brachytherapy sources on Monte

- Carlo simulations of kerma and dose rates in water and air. *Med Phys* 2010; 37: 869-876.
20. Badal A, Sempau J. A package of Linux scripts for the parallelization of Monte Carlo simulations. *Comput Phys Commun* 2006; 175: 10.
 21. Williamson JF. Monte Carlo evaluation of kerma at a point for photon transport problems. *Med Phys* 1987; 14: 567-576.
 22. Perez-Calatayud J, Granero D, Ballester F. Phantom size in brachytherapy source dosimetric studies. *Med Phys* 2004; 31: 2075-2081.
 23. Papagiannis P, Angelopoulos A, Pantelis E et al. Monte Carlo dosimetry of ^{60}Co HDR brachytherapy sources. *Med Phys* 2003; 30: 712-721.
 24. Selvam TP, Sahoo S, Vishwakarma RS. Comment on "Monte Carlo dosimetry of ^{60}Co HDR brachytherapy sources" [*Med Phys* 30, 712-721 (2003)]. *Med Phys* 2010; 37: 5146-5147.
 25. Selvam TP, Bhola S. Technical note: EGSnrc-based dosimetric study of the BEBIG ^{60}Co HDR brachytherapy sources. *Med Phys* 2010; 37: 1365-1370.
 26. Hariri Tabrizi S, Kamali Asl A, Azma Z. Monte Carlo derivation of AAPM TG-43 dosimetric parameters for GZP6 Co-60 HDR sources. *Phys Med* 2012; 28: 153-160.